Effect of multiple firings on shear bond strength of feldspathic porcelain to base metal alloys: An in-vitro study

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ABSTRACT:
Background: The objective of the present study was to evaluate the effect of repeated firings on the metal-ceramic bond strength of cast Ni-Cr and Co-Cr alloy. Materials and Methods: Feldspathic porcelain (VITA VM13 Zahnfabrik, Bad Sackinger, Germany) was fused to Ni-Cr alloy (Wiron 99, Bego) and Co-Cr alloy (Wirolbond C, Bego). Thirty cylindrical specimens were cast for each alloy. Feldspathic porcelain was applied on the upper surface of the cylinders and fired according to manufacturers' instructions. In each group, specimens were divided into 3 subgroups based on repeated firings (3, 5, 7). Shear bond strengths were determined in a universal testing machine (INSTRON 3366, Norwood, USA), with a 2500-kgf load cell and crosshead speed of 1 mm/min, using a custom made steel apparatus. Failure loads were statistically analyzed first with the one-way ANOVA, and then compared with the Student t test. Results: One-way ANOVA test results showed no statistical differences between the metal-ceramic bond strength of Ni-Cr alloy (P = 0.127) and Co-Cr alloy (P = 0.087) after firing 3, 5, and 7 times. The mean shear bond load (N) for Ni-Cr alloy group (860.58 ± 40.81) was significantly higher (p=0.001) than Co-Cr alloy group (679.18 ± 43.31). Conclusion: The mean shear bond strength for the metal ceramic systems tested were not significantly affected by multiple firings and were considered as clinically acceptable for metal-ceramic restorations.

Key words: base-metal alloys, multiple firings, metal-ceramic alloys, shear bond strength.

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INTRODUCTION

Metal-ceramic restorations have been used in dentistry for over a century due to their excellent fracture resistance. Currently, base metal alloys have replaced the high noble and noble metal casting alloys by allowing fabrication of long span and cantilevered FPDs with lesser thickness and greater rigidity. Moreover, higher melting range reduces the risk of distortion and sagging of metal substructure during porcelain firing. Due to optimal mechanical properties, low density and cost considerations, base metal alloys are considered as a viable alternative to precious alloys in metal-ceramic restorations. However, restoration's longevity depends on the bond strength between the metal core and the veneering porcelain. Residual stress gradients, interfacial chemistry, and the interfacial morphology are the main factors that influence the success of a ceramic-metal bond.
Multiple firing procedures are usually necessary for the fabrication of metal-ceramic restorations to match the esthetics of natural dentition, especially when using the standard layering technique. It has been found that repeated firings of the base metal alloys enhance the formation of excessive oxide layers which could lead to fracture through the metal oxide. Furthermore, repeated firings may also produce changes in micro-crack density and partial decoupling of the leucite from the surrounding glass matrix, resulting in a lowering of the bulk thermal expansion of the porcelain. Large differences in thermal expansion coefficients may form residual stress gradients across the metal-ceramic interface during processing, with a subsequent decrease in bond strength. Therefore, the purpose of the present study was to determine the effect of repeated firings on the shear bond strength of feldspathic porcelain veneered to conventional cast base metal alloys.

**MATERIALS AND METHODS:**

Feldspathic porcelain (VMK 95, VITA Zahnfabrik, Bad Sackingen, Germany) was fused to two base metal alloys - Ni-Cr alloy (Wiron-99, Bego Ltd., Germany) and Co-Cr alloy (Wirobond-C, Bego Ltd., Germany) to form two porcelain-metal groups (Table 1).

**Preparation of cast specimens:**

A metal die was prepared according to the sample dimensions (cylindrical rod, 8mm in height; and 4mm in diameter) specified by de Melo et al (Figure 1) and its silicone index (Polyvinyl siloxane, Aquasil soft putty, Dentsply) was used to standardize the waxed parts for formation of the metallic aspect of the specimen. Sixty wax molds were made using inlay wax (Bego, Germany) and invested in a phosphate bonded investment material (Bellasun, Bego). Casting was done using centrifugal casting machine (OKAY PLUS, Galoni, Italy), through the lost wax casting technique, to obtain thirty correspondent metallic portion of the specimens for each alloy (Ni-Cr alloy, Wiron-99, Bego; and Co-Cr alloy, Wirobond C, Bego). Metal surface treatment was performed by degassing and grit-blasting the specimens with aluminum oxide (100µ) under 2-bar pressure for 10 seconds (Model Microjet II, EDG, Sao Carlos, SP, Brazil). The specimens were cleaned with tap water, isopropyl alcohol and then allowed to dry for 10 minutes.

**Veneering procedure**

Two thin layers of opaque porcelain powder (VMK 95, VITA Zahnfabrik, Bad Sackingen, Germany) in a paste/liquid mix were applied on the metal specimens using a brush and fired according to the manufacturer's instructions (Porcelain furnace, Vacumat 40; VITA Zahnfabrik, Bad Sackingen, Germany). Dentin porcelain was condensed to a height of 4mm in a slightly oversized silicone putty index to compensate for the contraction generated during the first firing cycle (Figure 2) and submitted to dentin firing to achieve the final dimensions of the samples as described in Figure 1. The specimens within each group were randomly divided into three subgroups and subjected to repeated firings as per manufacturers' instructions (Table 2).

**Testing Procedures**

The mechanical shear bond test was performed using a custom made steel apparatus consisting of two independent parts (A and B), that concentrated the tension at the metal-ceramic interface. The Part A was cylindrical with a flat interior adaptation that enabled insertion of the other Part B, comprising of an upper cylindrical prolongation to serve as a piston during the mechanical evaluation of the specimens (Figure 3). The specimens were inserted into the apparatus through an orifice (4mm diameter) on the flat side of both the parts, that lodged the metallic portion of the specimen in Part A and the ceramic portion in Part B (Figure 4). The shear bond test was conducted in a universal testing machine (INSTRON 3366, Norwood, USA), with a 2500-kgf load cell that applied shear forces at the metal-porcelain interface at a crosshead speed of 1 mm/min until failure occurred. Failure loads were recorded in Newton (N) and results were converted into MPa using the following formula:

\[
\text{Stress (MPa)} = \frac{\text{Load}}{\pi r^2} = \frac{12.56}{3.14 \times 4} \approx 3.14 \times 4 = 12.56 \text{ (mm}^2\text{)}
\]

**Statistical Analysis**

One-way ANOVA test was used (p<0.05) for statistical analysis of the data. The mean values of the two groups were compared using student’s t test. A statistical software package (SPSS 15.0; SPSS, Inc., Cary, NC, USA) was used for the analysis.
RESULTS

The mean bond strength values and standard deviations using the one-way ANOVA test are presented in Table 3 and 4. Results showed no statistically significant difference between shear bond strength values in the Ni-Cr/porcelain and Co-Cr alloy/porcelain combinations (p=0.05) after 3, 5 and 7 repeated firings. The Student t test results showed that Group A (68.52 MPa ± 40.81) had significantly higher mean shear bond strength value than Group B (54.07 MPa ± 43.31) (Table 5).

DISCUSSION

The suitable oxidation of metal and interdiffusion of ions between the metal and porcelain is believed to be the main adhesion mechanism in PFM restorations. Base metal alloys with nickel and chromium, form excessive oxide layers that may increase the risk of porcelain fracture. Mclean demonstrated that the coefficient of thermal expansion of vita porcelain was decreased due to nickel and chromium oxide and induced stresses, leading to failure of the non-precious metal-ceramic restorations. The thickness of oxide layer formed during the oxidation process depends on the alloy composition, preparation of metal and length of firing. It is common laboratory practice to remove some of the oxides before porcelain application by means of grit-blasting after de-gassing. Pask and Tomsia found that the amount of Ni2O and Cr2O3 was less at the metal-porcelain interface in the argon fired specimens than in the vacuum-fired ones. Barghi et al measured the fracture strength of repeatedly fired porcelain veneered to high noble and base metal alloy crowns and reported that multiple firings decreased the fracture strength in high noble alloys but did not significantly affect base metal alloys. The Selective laser melting (SLM) metal ceramic system showed improved porcelain adherence compared with conventional cast methods after 5 and 7 firings.

In the present study, cast Ni-Cr and Co-Cr alloy were used to investigate the metal-ceramic bond...
strength after multiple firings. Various tests
designed by researchers to evaluate bond strengths
of different metalloceramic systems can be classified
according to the nature of stresses created such as
shear, tensile, flexural strength, torsion or a
combination of the previous.20 Although, no single
test method can be universally considered to be the
most valid for clinical implications, shear tests are
widely used because of its relative simplicity of use,
ease of specimen preparation and rapid production
of test results.21, 22  The base metal alloys mostly
indicate a predominance of interface failures,
suggesting a weak oxide layer at the metal-ceramic
interface.23 Therefore, in the present study shear
bond strength was tested through a custom made
apparatus to direct the tension mostly to the metal-
ceramic interface. Although, different values of bond
strength are expected with different testing modes,
the minimum of 51 MPa has been suggested as lower
limit for bond strength.24 Multiple firings (3, 5 and
7) had no significant effect on shear bond strength
of both the test groups. The mean shear bond
strength of Ni-Cr alloy group (68.52 MPa) was
higher than the Co-Cr alloy group (54.07 MPa).
However, an advantage of Co-Cr alloys over Ni-Cr
alloys is its great biocompatibility relative to the
allergenic potential associated with beryllium and
nickel.25 Therefore, cobalt-chromium alloys can be
used as a suitable base-metal alternative for patients
allergic to nickel. Further evaluation of the effects
of other parameters such as different firing
temperatures and thermocycling immersion times,
on alternative alloys used in metal-ceramic
restorations is required before making any clinical
recommendations.

CONCLUSION

Within the limitations of this study, selected
cast base metal alloys and veneering porcelain
combinations were found to be suitable for clinical
use as repeated firings did not significantly affect
the metal-ceramic bond strength.

REFERENCES

1. Wataha JC. Alloys for prosthodontic restorations. J Prosthet
   Dent 2002; 87:351-63.
2. Jarad FD, Russell MD, Moss BW. The use of digital imaging
   for colour matching and communication in restorative
3. Wee AG, Chen WY, Johnston WM. Color formulation and
   21:665-70.

Table 1: Experimental groups division

<table>
<thead>
<tr>
<th>Group</th>
<th>Porcelain/Metal</th>
<th>Number of samples</th>
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</thead>
<tbody>
<tr>
<td>Group A</td>
<td>Vita VMK 95 /Ni-Cr</td>
<td>30</td>
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<tr>
<td>Group B</td>
<td>Vita VMK 95 /Co-Cr</td>
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Table 2: Experimental group subdivisions

<table>
<thead>
<tr>
<th>Group A subdivisions</th>
<th>Group B subdivisions</th>
<th>Repeated firing cycles</th>
<th>Number of samples</th>
</tr>
</thead>
<tbody>
<tr>
<td>A0</td>
<td>B0</td>
<td>3</td>
<td>10</td>
</tr>
<tr>
<td>A1</td>
<td>B1</td>
<td>5</td>
<td>10</td>
</tr>
<tr>
<td>A2</td>
<td>B2</td>
<td>7</td>
<td>10</td>
</tr>
</tbody>
</table>

Table 3: One-way ANOVA for mean shear bond loads between the Sub-groups of Group A

<table>
<thead>
<tr>
<th>Group A (Ni-Cr)</th>
<th>Mean</th>
<th>SD</th>
<th>P-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>A0</td>
<td>875.33</td>
<td>43.79</td>
<td>0.127</td>
</tr>
<tr>
<td>A1</td>
<td>866.59</td>
<td>40.28</td>
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<tr>
<td>A2</td>
<td>839.81</td>
<td>32.62</td>
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Table 4: One-way ANOVA for mean shear bond loads between the Sub-groups of Group B

<table>
<thead>
<tr>
<th>Group B (Co-Cr)</th>
<th>Mean</th>
<th>SD</th>
<th>P-value</th>
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<tbody>
<tr>
<td>B0</td>
<td>702.17</td>
<td>34.83</td>
<td>0.087</td>
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<tr>
<td>B1</td>
<td>674.94</td>
<td>42.94</td>
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<tr>
<td>B2</td>
<td>660.42</td>
<td>44.60</td>
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</table>

Table 5: Comparison of Mean shear bond loads between Group A & Group B using student-t test

<table>
<thead>
<tr>
<th>Group</th>
<th>Mean</th>
<th>SD</th>
<th>p-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>A (Ni-Cr)</td>
<td>860.58</td>
<td>40.81</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>B (Co-Cr)</td>
<td>679.18</td>
<td>43.31</td>
<td></td>
</tr>
</tbody>
</table>

SD: Standard deviation


